## MODELLING BIOLOGICAL MACROMOLECULES IN SOLUTION: THE GENERAL TRI-AXIAL ELLIPSOID

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## CHAPTER 3

Numerical Inversion Procedures:

The Problem of the Line Solution

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#### 3.1 Solution of the Elliptic Integrals

In order to determine the viscosity increment  $\nu$  that corresponds to a particular value of the axial ratios a/b, b/c, the elliptic integrals  $\alpha_0$  etc. (Appendix I) must be solved. Analytic solutions are not possible but the integrals can be solved numerically with the aid of a high speed computer. The subroutine used for this was the United Kingdom NAG Mk. 6 routine DO1AGF which evaluates a definite integral of the form

$$I = \int_{A}^{B} f(t) dt$$

where A=0, using an interval subdivision strategy developed by Oliver (1972) and based on Clenshaw-Curtis quadrature (1960). Since infinity cannot be used as the upper limit, a finite value of 8 must be specified. However, a satisfactory value for 8 can be determined by using successively higher values until the value of the integral converges to a limiting value; in this case a value for 8 of 10<sup>6</sup> was sufficient. Higher values are also suitable although evaluation of the integral takes longer. The number of interval subdivisions is also specifiable by the user; the maximum number of 50 was used. The routine also estimates the error on the integrals (0'Hara & Smith, 1968). If this error is greater than the maximum allowable error specifiable by the user the routine will stop and print an error message. The maximum allowed absolute error specified was 1.0 × 10<sup>-8</sup> (=.001%). The subroutine for evaluating the elliptic integrals can easily be incorporated into a program for evaluating  $\nu$  for a given value of (a/b, b/c). This is given in Appendix V as Program 1.

# 3.2. Application to the Crystallographic Dimensions of Myoglobin; Numerical Inversion

The result can be applied to crystallographic data available for myoglobin. Kendrew et al (1958) gave the dimensions of sperm whale myoglobin to be  $43 \times 35 \times 23$  Å (Table 3). This corresponds to a general tri-axial ellipsoid of semi-axes a = 21.5, b = 17.5 and c = 11.5 Å, and axial ratios a/b = 1.23, b/c = 1.52. Using Program 1 (Appendix V) this corresponds to a viscosity increment of 2.729. The predicted intrinsic viscosity can then be found from equation (8):

$$[n] = v \overline{v}_{S} \equiv v \overline{v} \left( \frac{\overline{v}_{S}}{\overline{v}} \right)$$
(92)

where  $(\overline{v}_s/\overline{v})$  is the swelling ratio (section 1.7.1). By fitting data of reduced specific viscosity against concentration (Table 8, Figure 27) I have determined the intrinsic viscosity of myoglobin to be  $(3.25 \pm .05)$  ml/gm, using a weighted least squares analysis (straight line fit). The concentrations were determined using a high precision auto density meter (Kratky et al, 1969, 1973) together with a  $\overline{v}$  for myoglobin of .741 ml/gm (Theorell, 1934):

$$c_{i} = \frac{\rho_{i} - \rho_{o}}{1 - \overline{\nu}\rho_{o}} \tag{93}$$

where  $\rho_0$  is the solvent density and  $\rho_1$  the solute densities. Use of the auto density meter, which is based on the time taken to perform a preset number of oscillations of a U-tube filled with the sample has the added advantage that, besides being very accurate, only small amounts of fluid are required (~1 ml). The experimental arrangement used for the viscosity and densimetric work is illustrated in Figure 28. The

platinum resistance thermometer shown was used to monitor the sample temperatures to accuracies of .005 degrees and was calibrated by myself. In order that the crystallographic dimensions gives this same value for [n], from equation (92), a swelling ratio  $(\overline{v}_s/\overline{v})$  of 1.6 is required; alternatively myoglobin is more asymmetric in solution.

In order to determine the actual dimensions of the equivalent triaxial ellipsoid for myoglobin in solution (or any other macromolecule) from the experimental value for [n], the situation is more complicated however. Although equation (88) defines a unique value of v for a given value of (a/b, b/c), an analytic inversion of (88) to produce an explicit expression for (a/b, b/c) in terms of v is not available. The inversion must therefore be done numerically by tabulating, or better plotting  $\nu$  as a function of (a/b, b/c). The same subroutine mentioned in section 3.1. for evalueting the elliptic integrals may be incorporated. A perusal of Table 7 (produced from Program 2) reveals however that a given value of v does not correspond to a unique value of (a/b, b/c) but to a 'line solution' of possible values of (a/b, b/c). This is clearly illustrated in the contour plot (Figure 29) produced from Program 3 using GHOST graphical facilities where  $\nu$  is incremented from 2.5 to 7.0 in steps of 0.5. In order to determine a unique solution for (a/b, b/c) and hence the axial dimensions of a macromolecule in solution other hydrodynamic information must be used; we must therefore consider the translational and rotational frictional properties (section 1.2).

#### 3.3. Other Tri-axial Line Solutions

#### 3.3.1. The Translational Frictional Ratio; the $\beta$ and R Functions

It was previously stated in section 1.4. that although Perrin (1936) had provided an explicit formula for the translational frictional ratio of a general tri-axial ellipsoid in terms of the axial ratios (a/b, b/c), the elliptic integral in equation (12) could only be solved analytically for the special case of ellipsoids of revolution (i.e. two equal axes). However, since the elliptical integral is similar to those for the triaxial viscosity increment, it too can now be solved numerically using for example the subroutine discussed in section 3.1. A higher value for the upper limit, B was required:  $5 \times 10^7$ . A table of values of the Perrin function  $f/f_{c}$  ( $\equiv P$ ) for values of a/b and b/c was thus obtained (Table 9). Again, a perusal of the table reveals that a given value of P has a line solution of possible values of (a/b, b/c). However, in principle at least, by combining the line solution for P of a given macromolecule with the line solution for v, a unique solution for (a/b, b/c) can in principle be found from their intersection. This can be illustrated by assuming a particle of (a/b, b/c) = (1.5, 1.5), calculating the corresponding values for  $\nu$  and P using Program 1, and then plotting the line solutions using Program 4. Unfortunately Figure 30 reveals that the intersection for accuracies in v and P to four significant figures is very shallow, and allowing for ± 1% experimental error in each there is no intersection at all in the 'globular protein' range of the Figure. There is also the additional problem that in order to determine experimentally both  $\nu$  and P, knowledge is required of the swollen volume in solution.

However, now that  $\nu$  and P are available for tri-axial ellipsoids, then so should the  $\beta$  and R functions which do not require a knowledge of the swollen volume (equations 45 & 64). I have thus produced tables of these also (Tables 10 & 11); all four tri-axial functions so far mentioned viz  $\nu$ , P,  $\beta$  and R are plotted in Figure 31 allowing for  $\pm$  1% experimental error in each. There is still no reasonable intersection; the  $\beta$  function is, as expected, seen to be of little practical use as it is very sensitive to experimental error (the  $\beta$  - 1% line is completely off the map area). Of the 4 functions however, the R function is the most useful since it is relatively insensitive to experimental error and the experimental determination does not require a knowledge of the swollen volume (section 1.7.1.). In order to find a unique solution for (a/b, b/c) therefore, this should ideally be combined with a rotational frictional or relaxation tri-axial shape function which should satisfy the following criteria:

- (i) provides a suitable intersection with R
- (ii) is relatively insensitive to experimental error but sensitive to axial ratio
- (iii) is experimentally measurable to a high precision with currently available apparatus and data analytic techniques and
- (iv) does not require a knowledge of the swollen volume for its experimental determination.

### 3.3.2. The Rotational Frictional, Diffusion and Relaxation Line Solutions

For a tri-axial ellipsoid there will be three rotational frictional ratios  $\zeta_i/\zeta_0$  (i=a,b,c) corresponding to rotation about each of the three axes and hence three rotational diffusion ratios  $\theta_i/\theta_0$ . By analogy with the translational case in the previous section, although Perrin (1934) had

given explicit formula for the  $\zeta_i/\zeta_o$  in terms of (a/b, b/c), - eqn. (25), the elliptic integrals could only be solved analytically for the case of ellipsoids of revolution. The integrals can now be solved numerically, again utilising the routine described in section 3.1 (Programs 1,2 & 4). There is however no experimental technique for determining the rotational frictional or diffusion coefficients directly; rotational experiments determine rather relaxation time ratios. For example, the dielectric dispersion relaxation time ratios are related to the rotational frictional and diffusion ratios by equations (27). A plot of the rotational relaxation time ratio line solutions corresponding to (a/b, b/c) = (1.5, 1.5) is given together with the R function in Figure 32. Unfortunately, because of the difficulties raised in 1.5.1. resolution of the dielectric dispersion curve into the 3 relaxation times for a homogeneous solution of tri-axial ellipsoid particles is impossible in practice.

Whereas for ellipsoids of revolution there are three fluorescence anisotropy decay times (equation 42), for general tri-axial ellipsoids, there will be five (Cantor & Tao, 1971, Small & Isenberg, 1977) related to the three rotational diffusion coefficients by:

$$\tau_{1} = \frac{1}{3(\theta + \theta_{1})} \quad ; \quad \tau_{2} = \frac{1}{3(\theta + \theta_{2})} \quad ; \quad \tau_{3} = \frac{1}{3(\theta + \theta_{3})}$$

$$\tau_{4} = \frac{1}{2(3\theta - \Delta)} \quad ; \quad \tau_{5} = \frac{1}{2(3\theta + \Delta)}$$
(94)

where  $\theta=(\theta_1+\theta_2+\theta_3)/3$  is the mean rotational diffusion coefficient, and  $\Delta$  is defined by

$$\Delta = (\theta_1^2 + \theta_2^2 + \theta_3^2 - \theta_1\theta_2 - \theta_2\theta_3 - \theta_3\theta_1)^{\frac{1}{2}}$$

The fluorescence anisotropy relaxation time ratios  $\tau_j/\tau_0$  can thus be evaluated (equation 42, where j is now = 1,2,3,4,5); these have been tabulated by Small & Isenberg (1977) and are plotted in Figure 33, for (a/b, b/c) = (1.5, 1.5). Consideration of these functions however, at the moment at least, is purely academic; besides the problems cited in section 1.5.4., the necessary resolution of the decay curve into its four component exponentials (since  $\tau_5 \sim \tau_1$ ) is impossible (Small & Isenberg, 1977). Furthermore, since neither the fluorescence anisotropy decay time ratios nor the dielectric dispersion relaxation time ratios for tri-axial ellipsoids are of apparent use at the moment, the same must be true of their corresponding swelling independent functions, the explicit expressions in terms of axial ratio being obtainable from:

$$\delta_{i} = \frac{\zeta_{o}}{\zeta_{i}} v \qquad ; \qquad \mu_{i} = \left(\frac{f_{o}}{f}\right) \left(\frac{\zeta_{i}}{\zeta_{o}}\right)$$

$$(95, 96)$$

$$\gamma_{i} = \left(\frac{f}{f_{o}}\right)^{3} \frac{\rho_{o}}{\rho_{i}}$$
;  $\varepsilon_{i} = v \frac{\rho_{o}}{\rho_{i}}$  (97, 98)

$$\kappa_{j} = \nu \left(\frac{\tau_{o}}{\tau_{j}}\right) \qquad ; \qquad \xi_{j} = \left(\frac{f}{f_{o}}\right)^{3} = \frac{\tau_{o}}{\tau_{j}}$$
(99, 100)

where i=a,b,c and j=1,2,3,4,5. The relations for these functions in terms of experimental parameters have already been given in section 1.7.

Evaluation of the harmonic mean rotational relaxation time ratio in terms of axial ratio for tri-axial ellipsoids we can similarly obtain from

$$\frac{\tau_h}{\tau_o} = \frac{3}{\left(\frac{\varrho_o}{\varrho_a} + \frac{\varrho_o}{\varrho_b} + \frac{\varrho_o}{\varrho_c}\right)}$$

(101)

(Programs 1, 2 & 4, Figure 34). The corresponding swelling independent functions  $\Psi$  and  $\Lambda$  determined by combining with the translational frictional ratio and the viscosity increment respectively we can now also obtain from

$$\Psi = \begin{pmatrix} \frac{\tau_o}{\tau_h} \end{pmatrix} \begin{pmatrix} \frac{f}{f_o} \end{pmatrix}$$
 (102)

$$\Lambda = \left(\frac{\tau_o}{\tau_h}\right) v$$

(103)

(Programs 1,2 & 4, Figure 34). Unfortunately, these functions are generally very sensitive to experimental error, as Figure 35 illustrates; also the problems in determining the harmonic mean relaxation time raised in 1.5.4. still apply.

# 3.3.3 Electric Birefringence Decay: the $\delta_+$ and $\delta_-$ Functions

In section 1.5.2. we stated that Ridgeway (1966, 1968) has shown that the decay of electric birefringence for a homogeneous suspension of asymmetric macromolecules (e.g. tri-axial ellipsoids) would consist of two exponential terms:

$$\Delta n = \frac{N}{2n_{\ell}} \left\{ A_{+} e^{-6\theta_{+}t} + A_{-} e^{-6\theta_{-}t} \right\}$$
 (32)

where  $\Delta n$  is the birefringence, N the number density of particles in suspension and  $n_{\ell}$  the refractive index of the suspending medium. A<sub>+</sub> and A<sub>-</sub> are complicated functions depending on the initial orientation of the particles and their dielectric and diffusion properties. We may rewrite NA<sub>+</sub> /  $2n_{\ell}$  as A<sub>+</sub>, the 'pre-exponential factors'. Equation (32) then becomes:

$$\Delta n = A'_{+}e^{-6\theta_{+}t} + A'_{-}e^{-6\theta_{-}t}$$

(104)

 $\theta_+$  and  $\theta_-$  are related to the rotational diffusion constants  $\theta_i$  (and hence the rotational frictional coefficients since  $\zeta_i = kT/\theta_i$ ) by

$$\theta_{\pm} = \frac{1}{3} \sum_{i} \theta_{i} \pm \left\{ \left( \frac{1}{3} \sum_{i} \theta_{i} \right)^{2} - \frac{1}{3} \sum_{i>j} \theta_{i} \theta_{j} \right\}^{\frac{1}{2}}$$

$$(105a)$$

$$= \frac{kT}{3} \left\{ \sum_{i} \frac{1}{\zeta_{i}} \pm \left( \sum_{i} \frac{1}{\zeta_{i}^{2}} - \sum_{i>j} \frac{1}{\zeta_{i}\zeta_{j}} \right)^{\frac{1}{2}} \right\}$$
 (105b)

The dimensions of equation (105) are of energy/(volume x viscosity); we therefore 'reduce' it to a function of shape alone:

$$\theta_{\pm}^{\text{red}} \equiv \left(\frac{\eta_{0}}{kT}\right) V_{e} \theta_{\pm} = \frac{abc}{12} \left\{ \left(\frac{1}{\zeta_{a}^{"'}} + \frac{1}{\zeta_{b}^{"'}} + \frac{1}{\zeta_{c}^{"'}}\right) + \frac{1}{\zeta_{b}^{"'}}\right\}$$

$$\pm \left[ \left(\frac{1}{\zeta_{a}^{"'2}} + \frac{1}{\zeta_{b}^{"'2}} + \frac{1}{\zeta_{c}^{"'2}}\right) - \left(\frac{1}{\zeta_{a}^{"'}\zeta_{b}^{"'}} + \frac{1}{\zeta_{b}^{"'}\zeta_{c}^{"'}} + \frac{1}{\zeta_{c}^{"'}\zeta_{a}^{"'}}\right) \right]^{\frac{1}{2}} \right\}$$
 (106)

where

$$\zeta_{a}^{"} = \frac{b^{2} + c^{2}}{b^{2}\beta_{o} + c^{2}\gamma_{o}}; \quad \zeta_{b}^{"} = \frac{c^{2} + a^{2}}{c^{2}\gamma_{o} + a^{2}\alpha_{o}}; \quad \zeta_{c}^{"} = \frac{a^{2} + b^{2}}{a^{2}\alpha_{o} + b^{2}\beta_{o}}$$
(107)

The elliptic integrals  $lpha_{_{f O}}$  etc. are those defined by Jeffrey (1922) and are given in Appendix I.

A plot of the  $\theta_+^{\rm red}$  and  $\theta_-^{\rm red}$  functions, together with the R function corresponding to the point (a/b, b/c) = (1.5, 1.5) allowing for  $\pm$  1% experimental error is given in Figure 36. It is seen that the intersections are very reasonable (the  $\theta_+^{\rm red}$  - R intersection is nearly orthogonal) and the functions are relatively sensitive to axial ratio. However, experimental determination of  $\theta_\pm^{\rm red}$  requires of course knowledge of the swollen molecular volume in solution (equation 106). This can be conveniently eliminated however in the standard way by combining (106) either with the viscosity increment (8) or the translational frictional ratio (20b). If for example (106) is combined with the viscosity increment (8), swelling independent  $\delta_\pm$  functions are produced (Tables 12, 13, Figure 37):

$$\delta_{\pm} = 6\theta_{\pm}^{\text{red}} \quad v \equiv \frac{6}{N_{A}k} \left(\frac{\eta_{o}\theta_{\pm}}{T}\right) [\eta] M_{r}$$

(108)

where  $[\eta]$  is expressed in ml/gm. Alternatively,  $\theta_{\pm}^{\rm red}$  can be combined with the translational frictional ratio (20b) to give swelling independent  $\gamma_{\pm}$  functions (Programs 1,2,4, Figure 38):

$$\gamma_{\pm} = 6\theta_{\pm}^{\text{red}} \left(\frac{f}{f_0}\right)^3 \equiv \frac{M_r^3 (1 - \overline{\nu} \rho_0)^3 \theta_{\pm}}{27 N_A kT \pi^2 \eta_0^2 s^3}$$

(109)

The  $\delta_{+}$  and  $\gamma_{+}$  functions are new. The  $\delta_{+}$  functions are preferred over the  $\gamma_{+}$  functions since they require fewer experimental measurements and do not involve squared or cubed terms; hence in principle can be measured more

accurately. It is seen therefore that combination of the R-function with the  $\delta_{\pm}$  functions as a method for determining a unique solution for the axial ratios (and hence the axial dimensions, if  $V_{\rm e}$  is known from  $k_{\rm h}/k_{\rm s}$  - section 1.7.1) of a macromolecule in solution satisfies the criteria (i), (ii) and (iv) of section 3.3.1. In order for the method to satisfy criterion (iii) however, there still remains the problem of resolving the exponential decay term into its 2 component relaxation times or decay constants (the same is true of course for the  $\theta_{\pm}^{\rm red}$  and  $\gamma_{\pm}$  functions). To date this has not been possible. We now show that with a new 'constrained' least squares algorithm using intersection with the R-curve as the constraint, this is now possible with currently available experimental precision.

Table 8. Values of reduced specific viscosity for various concentrations of sperm whale myoglobin (0.1M NaCl buffer, pH = 7.1)

Concentration, c (mg/ml)	n <sub>rel</sub>	n <sub>sp</sub> /c (ml/gm)
90.2	1.450	4.99
66.1	1,298	4.51
53.3	1.224	4.20
50.2	1.215	4.29
40.7	1.163	4.00
34.4	1.138	4.02
30.5	1.116	3.81
29.6	1.115	3.89
23.2	1.084	3.61
15 <b>.5</b>	1.055	3.57
9.7	1.034	3.47
8.1	1.028	3.50

Table 9. Values of P as a function of (a/b, b/c) for a general tri-axial ellipsoid (a>b>c)

	b/c a/b	Prolate Ellipsoid										
	a/b	1.0	1.1	1.2	1.3	1.4	1.5	1.6	1.7	1.8	1.9	2.0
Oblate Ellipsoi	d 1.0	1.000	1,001	1.003	1.006	1.010	1.014	1,019	1.025	1.030	1.036	1.042
	1.1	1.001	1.002	1.005	1.009	1.014	1.019	1.024	1.030	1.036	1.042	1.049
	1.2	1.003	1.005	1.009	1.013	1.018	1.024	1.030	1.036	1.043	1.049	1.056
	1.3	1.006	1.009	1.013	1.018	1.024	1.030	1.037	1.043	1.050	1.057	1.064
	1.4	1.010	1.014	1.019	1.024	1.030	1.037	1.044	1.051	1.058	1.065	1.073
	1.5	1.015	1.019	1.024	1.031	1.037	1.044	1.051	1.059	1.066	1.074	1.082
	1.6	1.020	1.025	1.031	1.037	1.044	1.052	1.059	1.067	1.075	1.083	1.091
	1.7	1.026	1.031	1.037	1.044	1.052	1.060	1.068	1.076	1.084	1.092	1.101
	1.8	1.031	1.037	1.044	1.052	1.059	1.068	1.076	1.085	1.093	1.102	1.111
	1.9	1.038	1.044	1.051	1.059	1.067	1.076	1.085	1.093	1.102	1.111	1.120
	2.0	1.044	1.051	1.059	1.067	1.075	1.084	1.093	1,102	1.112	1.121	1.130

Table 10. Values of  $\beta \times 10^{-6}$  as a function of (a/b, b/c) for a general triaxial ellipsoid (a>b>c)

	b/c	Prolate Ellipsoid										
a	\P	1.0	1.1	1.2	1.3	1.4	1.5	1.6	1.7	1.8	1.9	2.0
Oblate Ellipsoid	1 1.0	2.111	2.112	2.112	2.113	2.113	2.114	2.115	2.116	2.117	2.117	2.118
	1.1	2.112	2.112	2.113	2.113	2.114	2.115	2.116	2.117	2.118	2.118	2.119
	1.2	2.112	2.113	2.114	2.114	2.115	2.116	2.117	2.118	2.119	2.120	2.121
	1.3	2.113	2.114	2.115	2.116	2.117	2.118	2.119	2.120	2.121	2.122	2.123
	1.4	2.114	2.115	2.117	2.118	2.119	2.120	2.121	2.123	2.124	2.125	2.126
	1.5	2.116	2.117	2.119	2.120	2.121	2.123	2.124	2.125	2.127	2.128	2.129
	1.6	2.118	2.119	2.121	2.123	2.124	2.126	2.127	2.129	2.130	3.131	2.132
	1.7	2.120	2.122	2.123	2.125	2.127	2.129	2.130	2.132	2.133	2.135	2.136
	1.8	2.122	2.124	2.126	2.128	2.130	2.132	2.134	2.136	2.137	2.139	2.140
	1.9	2.124	2.127	2.129	2.131	2.134	2.136	2.138	2.139	2.141	2.143	2.144
	2.0	2.127	2.130	3.132	2.135	2.137	2.139	2.141	2.143	2.145	2.147	2.149

Table 11. Values of R as a function of (a/b, b/c) for a general tri-axial ellipsoid (a>b>c)

	b/c a/b	- Prolate - Ellipsoid	1.1	1.2	1.3	1.4	1.5	1.6	1.7	1.8	1.9	2.0
Oblate Ellips	oid 1.0	1.600	1.598	1.592	1.583	1.573	1.561	1.548	1.535	1.521	1.507	1.494
	1.1	1.598	1.593	1.585	1.575	1.563	1.549	1.536	1.521	1.507	1.493	1.478
	1.2	1.592	1.585	1.575	1.563	1,549	1.535	1.520	1.505	1.490	1.475	1.460
	1.3	1.582	1.573	1.561	1.548	1.533	1.518	1,502	1.486	1.471	1.455	1.440
	1.4	1.570	1.559	1.546	1.531	1.515	1.499	1.483	1.466	1.450	1.435	1.419
	1.5	1.556	1.543	1.529	1.513	1.496	1.479	1,462	1.445	1.429	1.413	1.397
	1.6	1.540	1.526	1.511	1.494	1.476	1.459	1.441	1.424	1.407	1.391	1.375
	1.7	1.524	1.509	1.491	1.474	1.455	1.437	1.419	1.402	1.385	1.368	1.352
	1.8	1.507	1.490	1.472	1.453	1.434	1.416	1.398	1.380	1.362	1.346	1.330
	1.0	1.489	1.471	1.452	1.433	1.413	1.394	1.376	1.358	1.340	1.324	1.307
	2.0	1.471	1.452	1.432	1.412	1.392	1.373	1.354	1.336	1.318	1.302	1.285

Table 12. Values of  $\delta$  as a function of (a/b, b/c) for a general tri-axial ellipsoid (a>b>c)

	b	)/c	Prolate Ellipsoid										
	a/b		1.0	1.1	1.2	1.3	1.4	1.5	1.6	1.7	1.8	1.9	2.0
Oblate Ellip	osoid	1.0	2.500	2.541	2.568	2.582	2.588	2.586	2.579	2.568	2.555	2.539	2.522
		1.1	2,549	2.577	2.596	2.605	2,606	2.601	2.595	2.279	2.564	2.547	2.529
		1.2	2.599	2.624	2.641	2.648	2.648	2.642	2.632	2.619	2,604	2.587	2.570
		1.3	2.648	2.675	2.692	2,700	2.700	2,695	2.686	2.674	2.660	2.644	2.627
		1.4	2.699	2.729	2.748	2.757	2.759	2.756	2.748	2.737	2.724	2.710	2.694
		1.5	2 <b>.7</b> 52	2.785	2.807	2.818	2.823	2.821	2.815	2.806	2.795	2.781	2.767
		1.6	2.806	2.844	2.868	2.883	2.890	2.891	2.887	2.880	2.870	2.858	2.845
		1.7	2.863	2.905	2.933	2.951	2.961	2,965	2.963	2.958	2.949	2.939	2.927
		1.8	2.922	2.968	3.001	3.023	3.036	3.042	3.042	3.039	3.033	3.024	3.014
		1.9	2.983	3.035	3.071	3.097	3.113	3.122	3.125	3.124	3.120	3.113	3.104
		2.0	3.047	3.103	3.145	3.174	3.194	3,206	3.212	3.213	3.210	3.205	3.198

Table 13. Values of  $\delta$  as a function of (a/b, b/c) for a general tri-axial ellipsoid (a>b>c)

Ь	/c	Prolate Ellipsoid										
a/b	\	1.0	1.1	1.2	1.3	1.4	1.5	1.6	1.7	1.8	1.9	2.0
Oblate Ellipsoid	1.0	2.500	2.454	2.413	2.377	2.344	2.314	2.286	2.259	2.235	2.212	2.190
	1.1	2.445	2.410	2.372	2.337	2,305	2.274	2.246	2.220	2,195	2.172	2.151
	1.2	2.387	2.350	2.313	2.277	2.245	2.214	2.185	2.159	2.134	2.111	2.089
	1.3	2.326	2.286	2.248	2.212	2.178	2.147	2.118	2.091	2.066	2.043	2.021
	1.4	2.264	2.222	2.183	2.146	2.112	2.081	2.051	2.024	1.999	1.976	1.954
	1.5	2.203	2.160	2.119	2.082	2.048	2.016	1.987	1.961	1.936	1.913	1.892
	1.6	2.144	2.100	2.059	2.021	1.987	1.956	1.927	1.901	1.877	1.854	1.834
	1.7	2.087	2.042	2.001	1.964	1.930	1.899	1.871	1.845	1.822	1.800	1.780
	1.8	2.033	1.987	1.946	1.910	1.876	1.846	1.819	1.794	1.771	1.750	1.730
	1.9	1.981	1.936	1.895	1.859	1.826	1.797	1.770	1.746	1.724	1.703	1.685
	2.0	1.932	1.887	1.847	1.812	1.780	1.751	1.725	1.702	1.680	1.661	1.643

## Figure 27. Plot of reduced specific viscosity versus concentration for sperm whale myoglobin (0.1M NaCl,buffer, pH = 7.1)

The straight line is that due to a weighted least squares fit to  $\frac{\eta_{sp}}{c} = [\eta] \ (1 + k_{\eta}c)$  where  $[\eta] = 3.25 \ ml/gm$  and  $k_{\eta} = 5.9 \ ml/gm$ .

The weight used was  $\frac{1}{\text{concentration (mg/ml)}}$  (conc. < 40 mg/ml)

 $\frac{1}{40} \qquad (conc. \ge 40 \text{ mg/ml})$ 

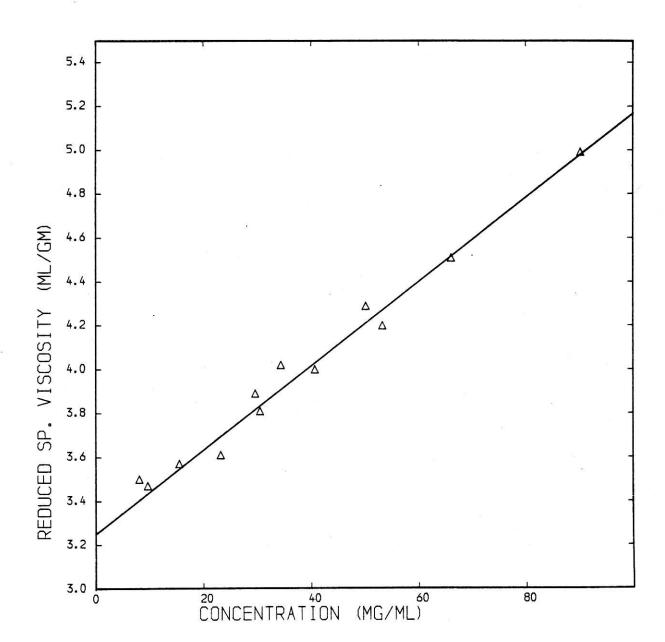
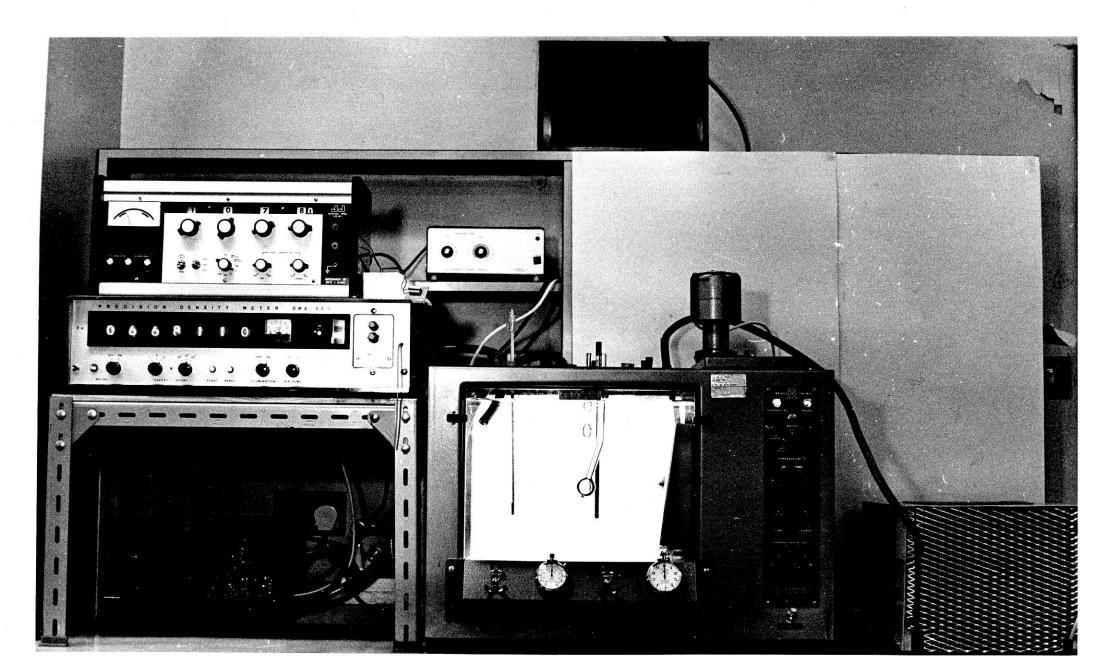


Figure 28. Photograph of the apparatus used for determining solution densities and viscosities. Temperatures were kept constant to within ± 0.01° using a high precision Townson - Mercer constant temperature tank, with a pump attachment to supply the water bath in the precision density meter. These temperatures could be monitored to within ± 0.005° using the platinum resistance thermometer situated directly above the density meter.



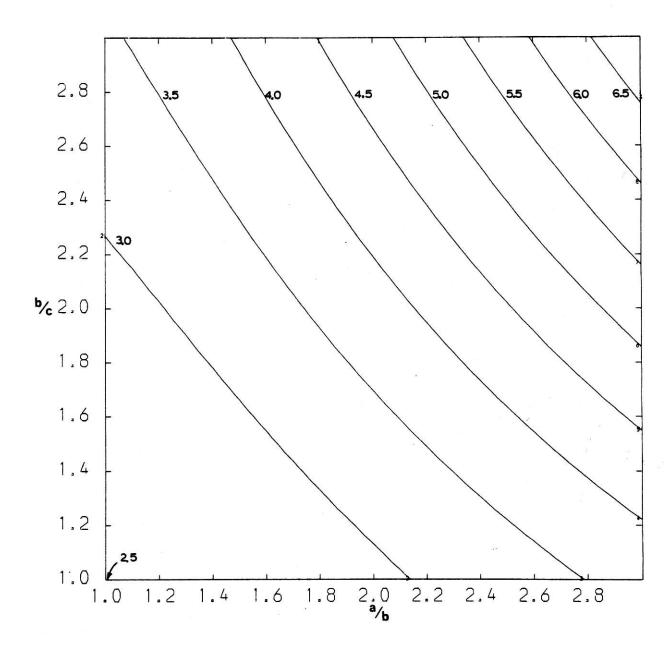


Figure 29. Contour diagram showing curves of constant v as a function of the semi-axial ratios a/b, b/c on the basis of equation (88)

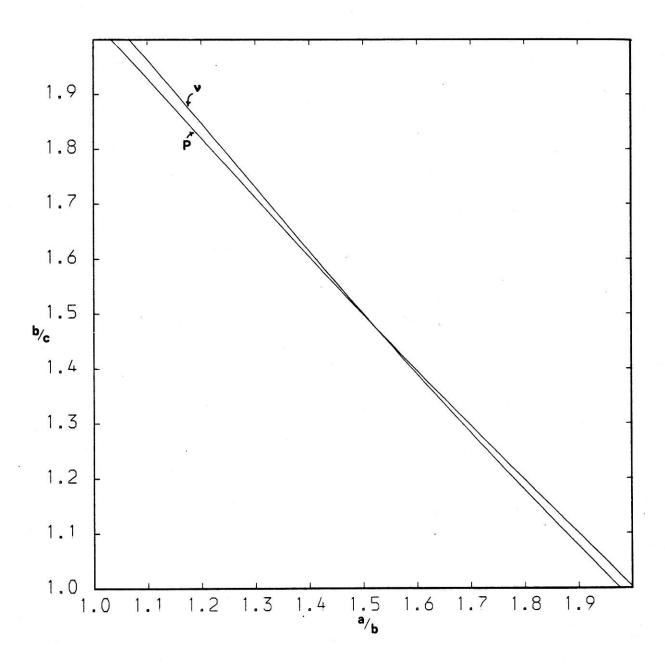


Figure 30. Plots of constant v and P in the (a/b, b/c) plane corresponding to a/b = 1.5, b/c = 1.5

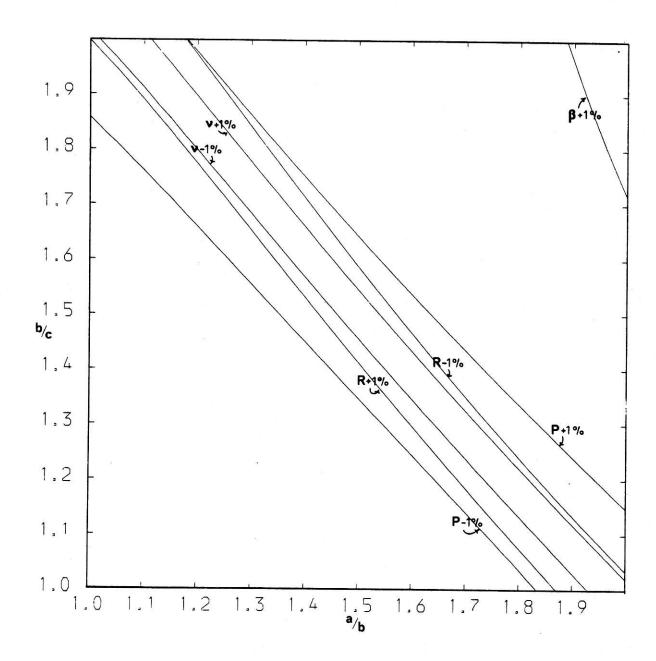


Figure 31. Plots of constant v, P,  $\beta$  and R, allowing for  $\pm$  1% error in their measured values, in the a/b, b/c plane corresponding to a/b = 1.5, b/c = 1.5

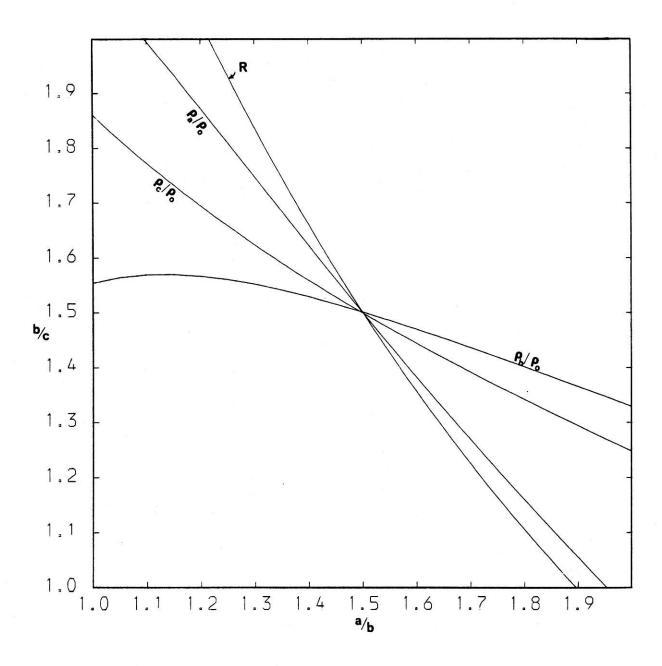


Figure 32. Plots of constant R and the rotational relaxation time ratios in the a/b, b/c plane corresponding to a/b = 1.5, b/c = 1.5

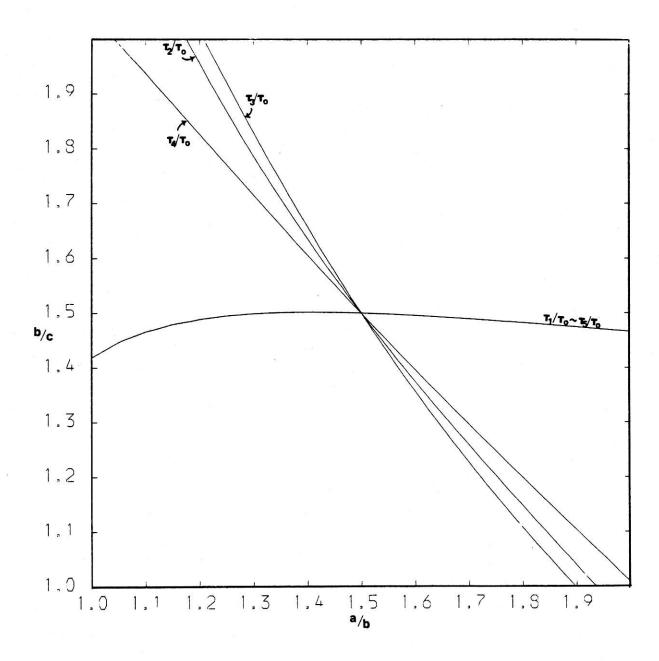


Figure 33. Plots of constant fluorescence anisotropy relaxation time ratios in the a/b, b/c plane corresponding to a/b = 1.5, b/c = 1.5

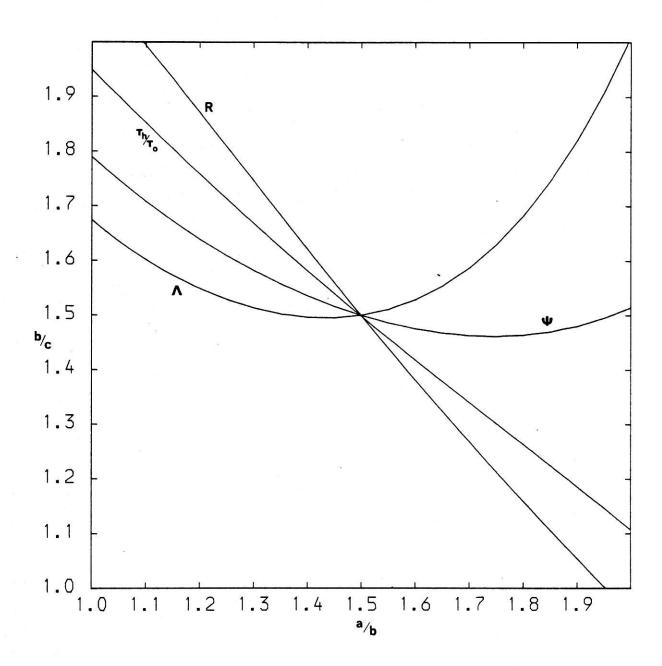


Figure 34. Plots of constant R,  $\Psi$  and  $\Lambda$  in the a/b, b/c plane corresponding to a/b = 1.5, b/c = 1.5

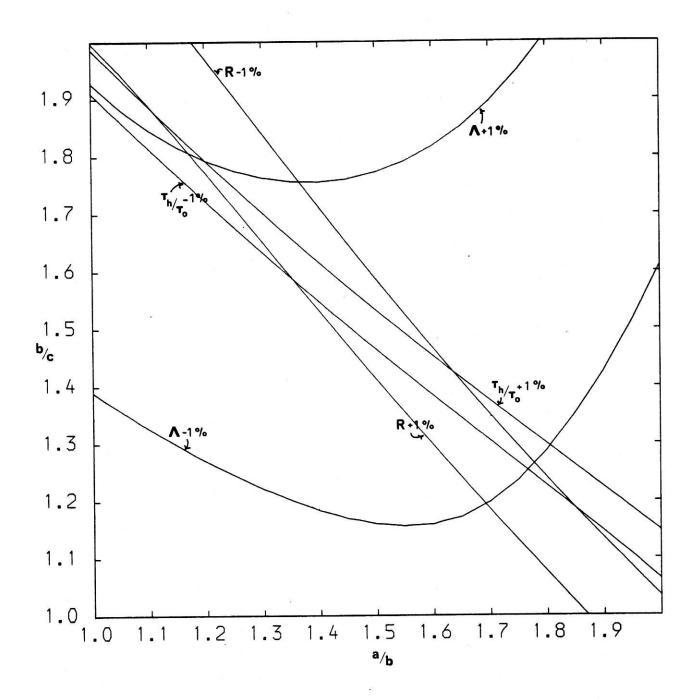


Figure 35. Plots of constant R,  $\Psi$  and  $\Lambda$ , allowing for  $\pm$  1% error in their measured values, in the a/b, b/c plane corresponding to a/b = 1.5, b/c = 1.5

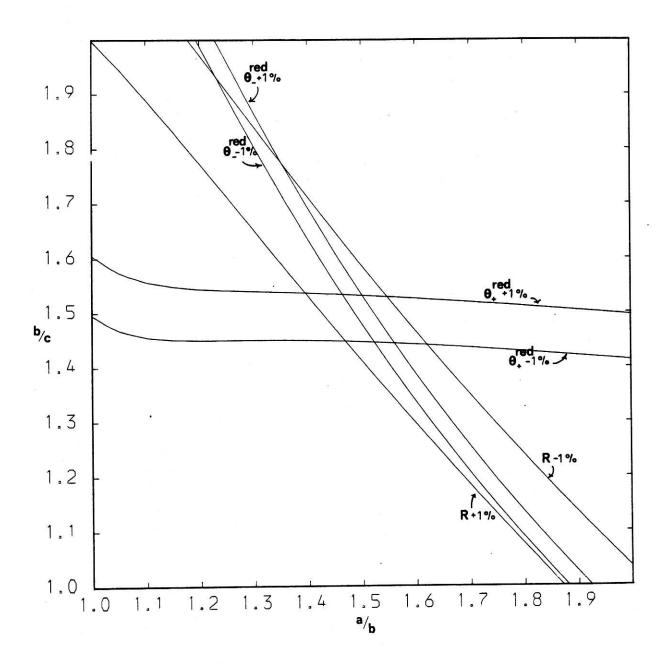


Figure 36. Plots of constant R,  $\theta_{+}^{\text{red}}$  and  $\theta_{-}^{\text{red}}$ , allowing for  $\pm$  1% error in their measured values, in the a/b, b/c plane corresponding to a/b = 1.5, b/c = 1.5

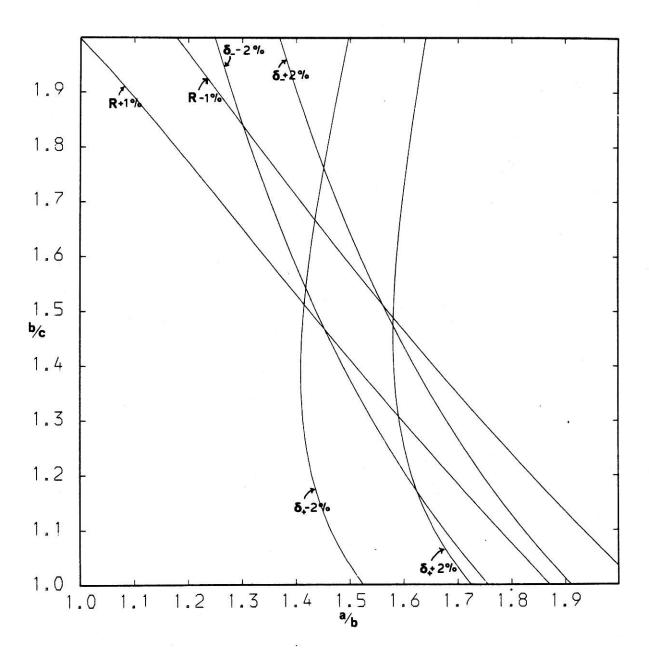


Figure 37. Plots of constant R,  $\delta$  and  $\delta$ , allowing for  $\pm$  1% measured error in R and  $\pm$  2% measured error in  $\delta$ , in the a/b, b/c plane corresponding to a/b = 1.5, b/c = 1.5

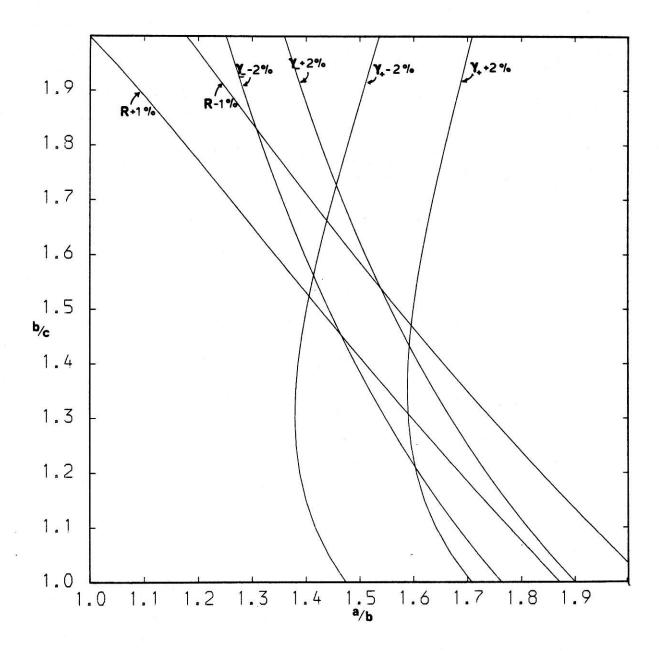


Figure 38. Plots of constant R,  $\gamma_{+}$  and  $\gamma_{-}$ , allowing for  $\pm$  1% measured error in R and  $\pm$  2% measured error in  $\gamma_{+}$ , in the a/b, b/c plane corresponding to a/b = 1.5, b/c = 1.5